

# INTEGRATED MECHANISMS OF $K^+$ LOSS IN MYOCARDIAL ISCHEMIA: A SIMULATION STUDY

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**Abstract**—During the early phase of myocardial ischemia, extracellular  $K^+$  accumulation is considered pivotal in the genesis of reentrant arrhythmias. Despite the importance of this phenomenon, the causes of cellular  $K^+$  loss are still unknown. Because of their ability to simulate the electrical activity of cardiomyocytes, action potential (AP) models provide an alternative for exploring their behavior under normoxic or pathological conditions. Our goal was to investigate, with the aid of computer simulations, the mechanisms responsible for the ischemic increase of extracellular  $K^+$  concentration ( $[K^+]_o$ ). The electrophysiological behavior of one single cardiomyocyte has been simulated during 14 minutes in the absence of coronary flow, using a modified version of Luo Rudy phase II AP model. The activation of the ATP- sensitive  $K^+$  current, as well as other possible causes of the ischemic increase of  $[K^+]_o$  such as inhibition of  $Na^+/K^+$  pump current and altered  $Na^+$  fluxes, have been taken into account in the simulations. Our results show that the concomitant effect of these three mechanisms in the absence of coronary flow leads to an increase of  $[K^+]_o$  quantitative and qualitatively similar to the experimentally observed during acute myocardial ischemia.

**Keywords** - Ischemia, extracellular  $K^+$  accumulation, causes.

## I. INTRODUCTION

Because of the frequent appearance of reentrant arrhythmias, the first minutes after the interruption of coronary flow are the most dangerous for cardiac tissue. The lack of oxygen and glucose leads to important changes in cellular metabolism and in the permeability of cell membranes. As a consequence, ionic concentrations are also modified and, more specifically, extracellular  $K^+$  concentration ( $[K^+]_o$ ) increases very early after the onset of myocardial ischemia.

Experimental reports show that the time course of  $[K^+]_o$  is of triphasic nature [1]. Several seconds after the interruption of coronary flow,  $[K^+]_o$  progressively increases until it reaches a plateau phase during which it remains almost constant for several minutes. Finally, a slower second rise takes place, simultaneously with a stopped glycolytic activity and cell death. The first increase of  $[K^+]_o$  lasts 10-15 minutes and corresponds to the early phase of myocardial ischemia. During this period, maximal levels of  $[K^+]_o$  could reach values as high as 18mM.

This extracellular  $K^+$  accumulation is related to electrophysiological changes in cardiac tissue that have been proved to be a main cause of reentrant arrhythmias [2]. During 20 years, several experimental groups have tried to determine the precise mechanisms that make myocytes lose  $K^+$  during acute myocardial ischemia. However, the causes of this arrhythmogenic factor remain uncertain. In this way, the simulation of action potential models could be an alternative tool to complete these investigations.

Because of its ability to simulate the electrophysiological behavior of ventricular cardiomyocytes, a modified version of Luo- Rudy phase II action potential model has been used to study the effect of several factors of myocardial ischemia on  $[K^+]_o$  in one single ventricular myocyte. The activation of the ATP- sensitive  $K^+$  current ( $I_{K(ATP)}$ ), the inhibition of  $Na^+/K^+$  pump current ( $I_{NaK}$ ) or an enhanced  $Na^+$  influx have been proposed to be the most probable among the possible causes of cellular  $K^+$  loss during ischemia [1, 3]. The goal of this work was to determine the effect of ischemia- induced changes in these three mechanisms of ionic transport on  $[K^+]_o$  in one single ventricular myocyte in the absence of coronary flow.

## II. METHODOLOGY

A modified version of Luo- Rudy phase II action potential model [4] has been used to simulate the electrophysiological behavior of one single cardiomyocyte, during 14 minutes of interrupted coronary flow. Four factors of myocardial ischemia have been considered in our simulations and their time course is described in Fig. 1.

A formulation of  $I_{K(ATP)}$  was incorporated into the model [5]. To simulate its activation during ischemia, the fraction of opened ATP- dependent  $K^+$  channels ( $f_{ATP}$ ) was increased in a linear manner from zero to a final value of 0.84% during 14 minutes of interrupted coronary flow.

Inhibition of  $Na^+/K^+$  pump activity was simulated by substituting the maximal current ( $I_{NaKMAX}$ ) by the expression:

$$I_{NaKMAX}(t) = I_{NaKMAX\_INI} \cdot [1 - f_{INHIB}(t)] \quad (1)$$

where  $I_{NaKMAX\_INI}$  is  $2.75\mu A/\mu F$  (the normoxic value of  $I_{NaKMAX}$ ) [4] and  $f_{INHIB}$  is the inhibition degree of  $Na^+-K^+$  pump.  $f_{INHIB}$  progressively increased from zero to its final value 35%, in accordance with experimental observations [6].

During myocardial ischemia, altered  $Na^+$  fluxes could lead to a  $Na^+$  leak current [3], represented in our simulations by the new  $Na^+$  current ( $I_{ONa}$ ). The amplitude of this current was linearly increased from zero to its final value  $-1.2\mu A/\mu F$ . In accordance with experimental results, its activation begins two minutes later than the changes in  $I_{K(ATP)}$  and in  $I_{NaK}$  [7,8].

The onset of myocardial ischemia leads to the absence of ionic flow between the interstitial space (cleft) and the bulk extracellular medium. This phenomenon was simulated by steeply increasing the time constant for diffusion of ions ( $\tau_{diff}$ ) from its normoxic value 1000ms to  $10^8$  ms, as described in Fig. 1. In order to stabilize ionic concentrations,  $\tau_{diff}$  was increased one minute before the beginning of alterations in  $I_{K(ATP)}$  and in  $I_{NaK}$ .

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To investigate the effect of simulated ischemia on unidirectional  $K^+$  fluxes, we monitored the number of  $K^+$  ions transported into and out of the cell,  $n_{IKout}$  and  $n_{INaK}$  respectively, which are defined as:

$$n_{IKout}(t) = \int_0^t I_{Kout} d\hat{o} \quad (2)$$

$$n_{INaK}(t) = \int_0^t I_{NaK} d\hat{o} \quad (3)$$

Then,  $divn_{IKout}(t)$  and  $divn_{INaK}(t)$  were computed as:

$$divn_{IKout}(t) = \frac{n_{IKout}(t) - n_{IKout}(60s)}{n_{IKoutNORM}(t) - n_{IKoutNORM}(60s)} \quad (4)$$

$$divn_{INaK}(t) = \frac{n_{INaK}(t) - n_{INaK}(60s)}{n_{INaKNORM}(t) - n_{INaKNORM}(60s)} \quad (5)$$

where  $n_{IKoutNORM}(t)$  and  $n_{INaKNORM}(t)$  are, respectively,  $n_{IKout}(t)$  and  $n_{INaK}(t)$  under normoxic conditions but in the absence of coronary flow

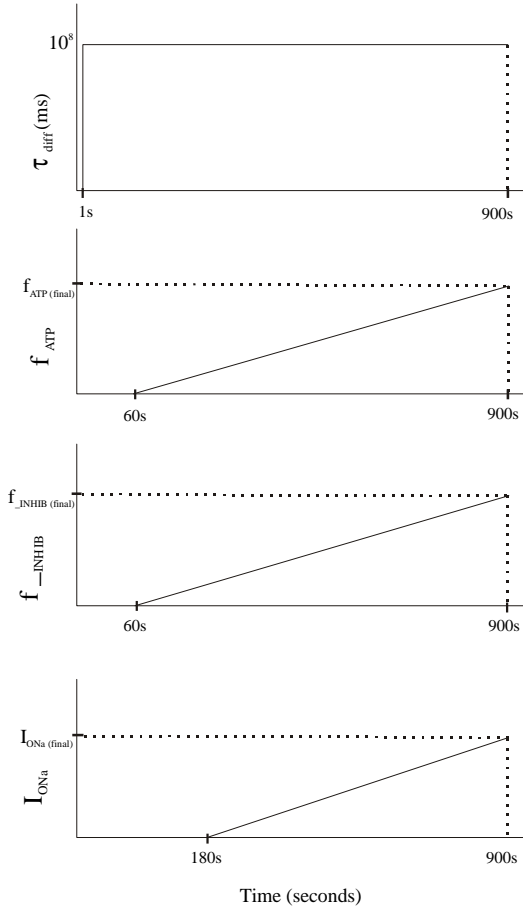


Fig. 1. Time course of ischemia- induced changes in ionic currents.

The model used in the simulations considers the three following compartments: the intracellular space, the interstitial extracellular clefts and a bulk extracellular medium in which concentrations were assumed to be constant. Dynamic changes in the extracellular (cleft) concentration of each ionic specie  $S$  ( $[S]_o$ ) are simulated with the equation [5]:

$$\frac{d[S]_o}{dt} = -\frac{A_m}{V_{cleft}F} I_{S,tot} - \frac{[S]_o - [S]_{bulk}}{\tau_{diff}} \quad (6)$$

where  $A_m$  is the area of the myocyte,  $V_{cleft}$  is the volume of the interstitial cleft (per cell),  $F$  is the Faraday constant,  $I_{S,tot}$  is the total ionic current associated to ion  $S$ ,  $\tau_{diff}$  is the time constant for diffusion of  $S$  from the interstitial clefts to the bulk extracellular medium, and  $[S]_{bulk}$  is the  $S$  concentration in the bulk.

The frequency of stimulation was 90 bpm that corresponds to a basic cycle length (BCL) of 666ms. The model was written in ACSL language. The nonlinear system of different equations was solved using the Gear stiff method. A maximum time step of 0.01ms was allowed.

### III. RESULTS

#### A. Extracellular $K^+$ accumulation during simulated ischemia.

As specified above, ischemia- induced alterations of three mechanisms of ionic transport ( $I_{K(ATP)}$ ,  $I_{NaK}$  and  $I_{ONa}$ ) have been proposed to be at least in part responsible for cellular  $K^+$  loss during the first minutes of interrupted coronary flow. Computer simulations have been carried out to determine the contribution of these mechanisms to extracellular  $K^+$  accumulation. Fig. 2 summarizes the results of four different cases. Simulations A, B and C correspond to the activation of only one of the ischemic mechanisms in the absence of coronary flow, while simulation D considers the concomitant effect of the alteration of the three currents.

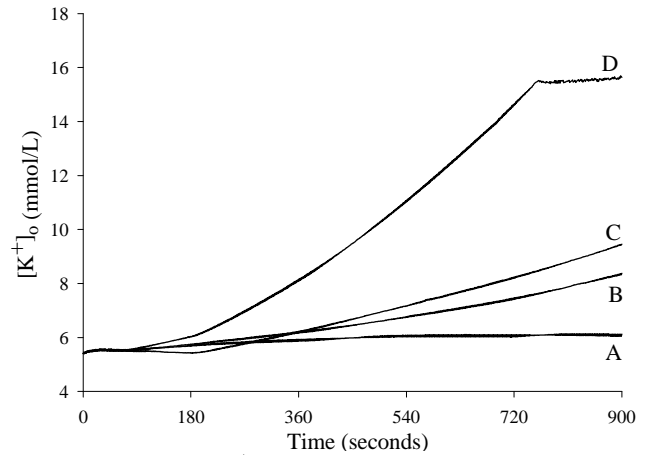


Fig. 2. Extracellular  $K^+$  accumulation during simulated ischemia.

Simulation A represents the slight increase of  $[K^+]_o$  during the progressive opening of  $K_{ATP}$  channels until  $f_{ATP}$  reaches a value of 0.84%. The final  $[K^+]_o$  is about 0.8mmol/L above its normoxic value (5.4mmol/L). Simulation B describes the time course of  $[K^+]_o$  for 14 minutes during which  $I_{NaKMAX}$  is decreased to 65% of its normoxic value. An extracellular  $K^+$  accumulation progressively takes place until a final  $[K^+]_o$  of 8mmol/L is reached. Finally, as shown in simulation C, the linear activation of  $I_{ONa}$  to  $-1.2\mu A/\mu F$  leads to a final  $[K^+]_o$  of 9.8mmol/L. Experimental reports show that the first increase of  $[K^+]_o$  is followed by a plateau phase with a final level that could reach 18mM [1]. Our simulations prove that the activation of only one of these mechanisms is not able to reproduce this extracellular  $K^+$  accumulation, neither quantitatively nor qualitatively.

Simulation D shows the integrated effect of the three mechanisms on  $[K^+]_o$  during 14 minutes of interrupted washout. The activation of  $I_{K(ATP)}$  simultaneous with  $Na^+/K^+$  pump inhibition is followed by a first rise of  $[K^+]_o$ , which is enhanced by the increase of  $I_{ONa}$ . Then, 11.6 min later,  $[K^+]_o$  reaches a plateau level of 15.5mmol/L and remains almost constant for the rest of the 14 minutes simulated.

#### B. Unidirectional $K^+$ fluxes during acute simulated ischemia.

Fig. 2 shows that only the integrated effect of changes in  $I_{K(ATP)}$ ,  $I_{NaK}$  and  $I_{ONa}$  leads to an increase of  $[K^+]_o$  similar to the experimentally observed during acute myocardial ischemia. In order to further investigate the causes of this cellular  $K^+$  loss, we have monitored the time course of  $divn_{INaK}$  and  $divn_{IKout}$ , both defined in Methods. These mathematical variables compare the number of  $K^+$  ions transported across the cell membrane during simulated ischemia with ionic fluxes under normoxic conditions. Thus, they provide interesting information about the consequences of simulated ischemia on unidirectional  $K^+$  fluxes. If  $divn_{INaK}$ , or  $divn_{IKout}$  is higher than one, then  $K^+$  influx or  $K^+$  efflux respectively has been reduced by the effect of the ischemic mechanisms considered. Fig. 3 depicts the time course of  $divn_{INaK}$  and  $divn_{IKout}$  under the conditions of simulated ischemia described in Fig. 1.

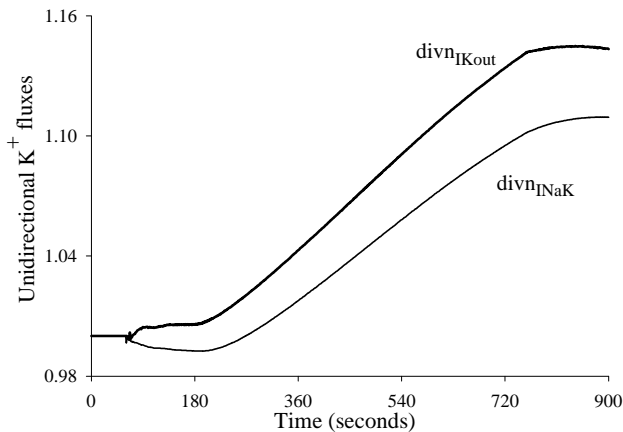


Fig. 3. Effect of simulated ischemia on unidirectional  $K^+$  fluxes.

As it can be observed, one minute after the interruption of coronary flow, the simultaneous effect of changes in  $I_{K(ATP)}$  and  $I_{NaK}$  produces a slight increase of  $divn_{IKout}$ . Two minutes later, the activation of  $I_{ONa}$  provokes a faster increase of  $divn_{IKout}$  that denotes an important enhancement of outward  $K^+$  current. During all the simulation,  $divn_{IKout}$  is higher than one, proving that the concomitant alteration of  $I_{K(ATP)}$ ,  $I_{NaK}$  and  $I_{ONa}$  in the absence of coronary flow increases unidirectional outward  $K^+$  flux. Three minutes before the end of the simulation, the slope of the curve changes and  $divn_{IKout}$  stabilizes in its final value 1.15. On the other hand, the time course of  $divn_{INaK}$  shows that, during the first two minutes of simulated ischemia, the linear decrease of  $I_{NaKMAX}$  reduces the ability of  $Na^+/K^+$  pump to transport  $K^+$  ions into the cell. Subsequently, a few seconds after the activation of  $I_{ONa}$ ,  $divn_{INaK}$  progressively increases up to 1, showing an enhancement of  $K^+$  influx despite the reduction of  $I_{NaKMAX}$ . As for  $divn_{IKout}$ , the slope of the curve decreases and at the end of the simulation the final value of  $divn_{INaK}$  was 1.10.

#### IV. DISCUSSION

Experimental reports have proved that extracellular  $K^+$  accumulation is in the origin of reentrant arrhythmias during acute myocardial ischemia. The importance of this phenomenon has involved a large number of investigators in the determination of the causes of cellular  $K^+$  loss. Even if the precise mechanisms are still unclear, their results suggest that opening of  $K_{ATP}$  channels, inhibition of  $Na^+/K^+$  pump activity and altered  $Na^+$  fluxes could play an important role in the ischemic increase of  $[K^+]_o$ .

In accordance with precedent studies from our group [9, 10, 11], our simulations show that the separate activation of only one of these mechanisms is not able to cause the extracellular  $K^+$  accumulation experimentally observed. However, their simultaneous alteration leads to a progressive rise of  $[K^+]_o$  followed by a plateau phase during which  $[K^+]_o$  remains almost constant. Qualitatively, this biphasic time course of  $[K^+]_o$  is typical of the first 10-15 minutes of myocardial ischemia [1]. Quantitatively, the rate of rise of  $[K^+]_o$  and the plateau level are in the range of those measured in cardiac tissues of pig, rabbit and guinea-pig. In conclusion, the simultaneous effect of the progressive change of  $I_{K(ATP)}$ ,  $I_{NaK}$  and  $I_{ONa}$  in the absence of coronary flow accurately reproduces the extracellular  $K^+$  accumulation observed during the early phase of myocardial ischemia.

During the first two minutes of simulated ischemia, the opening of  $K_{ATP}$  channels represents an increase of  $K^+$  permeability of cell membrane that could enhance  $K^+$  efflux and extracellular  $K^+$  accumulation. However, our results show that the single activation of  $I_{K(ATP)}$  produces a final extracellular  $K^+$  accumulation of 0.8mmol/L. A possible explanation of this small effect is that the opening of  $K_{ATP}$  channels increases  $K^+$  efflux across  $I_{K(ATP)}$  but also produces a faster repolarization of action potential. As a consequence, action potential duration is shortened and the time during which other  $K^+$  currents are activated is reduced. Furthermore, the  $I_{K(ATP)}$  enhancement of  $g_K$  not only produces

the shortening of APD but also a reduction of  $K^+$  driving force that would restrain outward  $K^+$  fluxes. Thus, extracellular  $K^+$  accumulation during ischemia could only be explained if this self-limiting effect of  $g_K$  is counteracted by an inward current.

The nature of this inward current is debated but experimental evidences have suggested that altered  $Na^+$  fluxes could contribute to cellular  $K^+$  loss [12]. In this way, the accumulation of substances like lysophosphatidylcholine has been proved to profoundly modify the characteristics of  $Na^+$  channels [13]. Their action during ischemia could result in a net  $Na^+$  inward current that could contribute to the increase of  $[Na^+]_i$  [7]. Simultaneously, this depolarizing current would enhance  $K^+$  driving force and cellular  $K^+$  loss during acute myocardial ischemia.

In accordance with this hypothesis, our results show that an inward current is necessary to explain the ischemic  $K^+$  accumulation in the extracellular space. The activation of  $I_{ONa}$  counteracts the effects of increasing  $f_{ATP}$  on APD and on  $K^+$  driving force and facilitates cellular  $K^+$  loss across  $I_{K(ATP)}$  and other  $K^+$  channels. Then, the concomitant effect of the opening of  $K_{ATP}$  channels and the activation of a  $Na^+$  inward current provokes a fast increase of unidirectional outward  $K^+$  flux.

In addition to the increase of  $K^+$  efflux, a decrease of  $Na^+/K^+$  pump ability to transport  $K^+$  ions would contribute to their accumulation in the extracellular space. In this way, experimental reports suggest that the pump could be partially inhibited by several ischemic factors like accumulation of inorganic phosphates, decreased intracellular pH and reduced intracellular ATP levels. However, other studies have shown that  $K^+$  influx persists and even is enhanced after the interruption of coronary flow [1].

Our results could explain this apparent discrepancy because, even if the  $I_{NaKMAX}$  is linearly decreased,  $K^+$  influx is only slightly reduced during the first minutes of simulated ischemia. Once the activation of  $I_{ONa}$  begins, the increase of  $[Na^+]_i$  and also of  $[K^+]_o$  is sufficient to enhance  $I_{NaK}$  despite the reduction of  $I_{NaKMAX}$ . Thus, in agreement with experimental observations,  $Na^+/K^+$  pump activity could play an important role on the onset of the plateau phase.

## V. CONCLUSION

The biphasic time course of  $[K^+]_o$  observed during the first 14 minutes of simulated ischemia is quantitative and qualitatively in accordance with the experimental data obtained during the acute phase of myocardial ischemia.

These results support the hypothesis that extracellular  $K^+$  accumulation could be caused by the concomitant effect of opening of  $K_{ATP}$  channels,  $Na^+/K^+$  pump inhibition and a net  $Na^+$  inward current in the absence of coronary flow. Cellular  $K^+$  loss results from an increase of unidirectional  $K^+$  efflux which is counteracted by an enhancement of  $Na^+/K^+$  current, possibly produced by changes in ionic concentrations.

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